

1 **Dental pulp-derived stem cell conditioned medium to regenerate peripheral nerves**
2 **in a novel animal model of dysphagia**

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14

15 **Abstract**

16 In nerve regeneration studies, various animal models are used to assess nerve regeneration.
17 However, because of the difficulties in functional nerve assessment, a visceral nerve
18 injury model is yet to be established. The superior laryngeal nerve (SLN) plays an
19 essential role in swallowing. Although a treatment for SLN injury following trauma and
20 surgery is desirable, no such treatment is reported in the literature. We recently reported
21 that stem cells derived from human exfoliated deciduous teeth (SHED) have a therapeutic
22 effect on various tissues via macrophage polarization. Here, we established a novel
23 animal model of SLN injury. Our model was characterized as having weight loss and
24 drinking behavior changes. In addition, the SLN lesion caused a delay in the onset of the
25 swallowing reflex and gain of laryngeal residue in the pharynx. Systemic administration
26 of SHED-conditioned media (SHED-CM) promoted functional recovery of the SLN and
27 significantly promoted axonal regeneration by converting of macrophages to the anti-

28 inflammatory M2 phenotype. In addition, SHED-CM enhanced new blood vessel
29 formation at the injury site. Our data suggest that the administration of SHED-CM may
30 provide therapeutic benefits for SLN injury.

31

32 **Introduction**

33 Peripheral nerve injury following trauma and surgery is a severe clinical problem that
34 results in potential long-term disability and a reduction in the patient's quality of life. In
35 peripheral nerve regeneration studies, the sciatic, facial, femoral and median nerves in
36 rodents and other larger animals are widely used to assess nerve regeneration [1]. For
37 clinical application, nerve-specific evaluation following several types of nerve injury is
38 necessary, but there are no previous reports on visceral nerve regeneration. Thus, an
39 animal model of visceral nerve lesion has not been established owing to difficulties in
40 assessing quantitative nerve function.

41 The superior laryngeal nerve (SLN) originates from the vagus nerve and plays an
42 important role in swallowing [2]. The SLN is a visceral sensory nerve that supplies the
43 pharyngeal and supraglottic mucosa [3]. Injury to the SLN during surgery, such as neck
44 dissection, thyroidectomy, anterior approaches to the cervical spine, or carotid
45 endarterectomy, causes dysphagia and subsequent aspiration pneumonia due to sensory
46 loss of the laryngopharynx and a reduction in the force of glottis closure [4]. Treatment
47 of SLN injury is not reported in the literature. Therefore, the development of effective
48 therapies for patients with dysphagia following SLN injury is necessary. However, there
49 are no reports regarding SLN regeneration owing to the lack of an evaluable experimental
50 animal model.

51 In recent years, researchers started investigating stem cell-based transplantation therapy
52 as a promising strategy for tissue regeneration. Stem cells from human exfoliated
53 deciduous teeth (SHEDs) and human dental pulp stem cells (hDPSCs) are self-renewing
54 mesenchymal stem cells derived from the perivascular niche of the dental pulp [5]. They

55 are thought to originate from the cranial neural crest that expresses early mesenchymal
56 and neuroectodermal stem cell markers [6-9]. They are able to maintain stemness
57 properties in 3D culture [10]. These stem cells are relatively easy to collect and exhibit
58 high plasticity and multi-potential capabilities [7]. We have previously shown that SHEDs
59 and hDPSCs transplantation in spinal cord injury promote the functional recovery of hind
60 limb movement [11]. Engrafting SHEDs facilitates successful peripheral nerve and
61 central nervous system regeneration in a paracrine fashion, activating intrinsic tissue-
62 repairing activities [12-14]. Transplantation of hDPSCs enhanced angiogenesis in sciatic
63 nerve resection and part of the stem cells differentiated into nerve cells [15, 16]. Our
64 studies have also shown that serum-free cultured conditioned medium (CM) from SHEDs
65 (SHED-CM) contains various factors that promote functional recovery after peripheral
66 nerve and central nervous system injury [17, 18]. Administration of CM avoids the
67 disadvantages of cell transplantation, such as tumorigenesis, strong immune reactions and
68 the difficulty in having a stable supply of cells. Furthermore, we have recently shown that
69 the SHED-CM promotes tissue regeneration by converting the macrophage phenotype
70 from pro-inflammatory M1 macrophages, which accelerate tissue destruction, to anti-
71 inflammatory M2 macrophages, which promote tissue repair [19].
72 The objective of this study was to validate a novel nerve injury model of SLN lesion in
73 the rat. Furthermore, we examined the therapeutic effects of intravenous administration
74 of SHED-CM in this model.

75

76 **Materials and methods**

77 **Study approval**

78 All experimental procedures involving animals were conducted in accordance with the
79 National Institutes of Health Guidelines for the Care and Use of Laboratory Animals, and
80 were approved by the Nagoya University School of Medicine Animal Care and Use
81 Committee. Exfoliated deciduous teeth from humans were collected under the guidelines

82 approved by Nagoya University (2015-0278). Ethical approval was obtained from the
83 Ethics Committee of Nagoya University (permission number 8-2). We obtained written
84 informed consent from all patients; in the case of minors, written informed consent was
85 given by their parents or guardians.

86

87 **Isolation of SHEDs and cell culture**

88 SHEDs were isolated as described previously [9]. In brief, human exfoliated deciduous
89 teeth were collected from patients aged 6–12 years. The dental pulp was separated from
90 the crown and root of the tooth. The isolated pulp was subsequently digested in a solution
91 of 3 mg/mL of collagenase type I and 4 mg/mL of dispase for 1 h at 37 °C. Single-cell
92 suspensions were cultured in Dulbecco's Modified Eagles' Medium (DMEM) (Gibco,
93 Rockville, MD) supplemented with 10% fetal bovine serum and with an antibiotic-
94 antimycotic solution (100 units/mL penicillin G, 100 mg/mL streptomycin, and 0.25
95 mg/mL amphotericin B; Gibco) and incubated at 37 °C in an atmosphere of 5% CO₂/ 95%
96 air. SHEDs used in this study exhibited a fibroblastic morphology with a bipolar spindle
97 shape, expressed MSC markers (CD90, CD73 and CD105) but not
98 endothelial/hematopoietic markers (CD34, CD45, CD11b/c or HLA-DR), and were
99 capable of undergoing adipogenic, chondrogenic and osteogenic differentiation [11].

100

101 **Preparation of CM**

102 After the SHEDs reached 80% confluency, the medium was replaced with serum-free
103 DMEM (DMEM (-)) containing the antibiotic-antimycotic solution. The cell-culture's
104 CM was collected after a 48-h incubation period. The CM was collected by centrifugation
105 for 5 min at 440 × g, and was centrifuged again for 3 min at 17,400 × g to remove cell
106 debris. We used the SHED-CM without either enrichment or dilution. The CM was
107 collected and stored at 4 °C before use in the following experiments.

108

109 **Animals**

110 All animal experiments undertaken in this study were performed in strict accordance with
111 the protocols approved by the Institutional Animal Care Committee. Male Wistar/ST rats
112 weighing 300-330 g (9–10 weeks old) were obtained from Japan SLC Shizuoka, Japan
113 Inc. All rats were maintained on a 12-h light/ dark cycle with free access to food and
114 water.

115

116 **Surgical procedures**

117 All rats were anesthetized using an intraperitoneal (i.p.) administration of a mixture of
118 medetomidine (0.15 mg/kg, i.p.; Domitor; Nippon Zenyaku Kogyo Co., Ltd., Fukushima,
119 Japan), midazolam (2 mg/kg, i.p.; Dormicum Astellas Pharma Inc., Tokyo, Japan) and
120 butorphanol (2.5 mg/kg, i.p.; Vetporphale Meiji Seika Pharma CO., Ltd., Tokyo, Japan).
121 Anesthetized rats were maintained at a constant temperature of 37 °C on a warming plate.
122 The neck skin was shaved and opened under a surgical microscope (Olympus, Tokyo,
123 Japan). The SLN was exposed bilaterally and injured with a vascular clip (60 g/mm²;
124 NATSUME SEISAKUSHO Co Ltd., Tokyo, Japan) over a period of 30 min. The muscle
125 and skin layers were closed with 4–0 Vicryl sutures (Ethicon Inc., Somerville, NJ). The
126 animals were randomly assigned to the following four groups: (1) Sham: SLN exposure
127 without any damage to the nerve tissue; (2) Injury: not injected; (3) DMEM (-): 1 ml
128 DMEM (-)-injected into the tail vein for 10 s simultaneously with the SLN damage; (4)
129 SHED-CM: 1 ml SHED-CM-injected into the tail vein for 10 s simultaneously with the
130 SLN damage.

131

132 **Measurements of food intake and body-weight**

133 Following SLN injury, the body-weight and food intake of rats were measured daily.
134 Animals had free access to food and water.

135

136 **Swallowing analysis**

137 Two weeks before the swallowing analysis, rats were placed in a custom-designed plastic
138 test cage (300 × 150 × 200 mm) twice per week for 2 h with free access to water in a
139 water bottle inclined at about 45 degrees, which was located 75 mm above the cage
140 bottom. At 7 days after surgery, after 16-h of water restriction, which was reported to
141 induce thirst [20, 21], each animal was placed in a test cage with free access to water.
142 Swallowing was recorded using a digital video camera (HDR-AS50; Sony, Tokyo, Japan),
143 and the volume of water intake was measured for 2 min. The videos were recorded at 120
144 frames per second and at a resolution of 1280 × 720. Video images were digitized for
145 frame-by-frame analysis using movie analysis software (PowerDirector 15; Cyberlink,
146 Tokyo, Japan), and the number of water intake interruptions and lick rate (lick cycle per
147 second) were measured. Lick rate started to be counted the first time the tongue was
148 maximally protruded at the spout, and each subsequent maximal tongue protrusion was
149 counted [20].

150

151 **Measurement of the swallowing reflex**

152 The method used for measuring the swallowing reflex was previously reported [3, 22, 23].
153 Briefly, at 7 days after surgery, the swallowing reflex was elicited experimentally by intra-
154 pharyngeal injection of distilled water. Animals were anesthetized with pentobarbital (40
155 mg/kg, i.p.), and then fixed in the supine position on a heated pad. A catheter was inserted
156 through the mouth, with its tip placed into the pharynx. The trachea of the animal was
157 cannulated to maintain respiration. Distilled water was applied to the pharyngolaryngeal
158 region twice, at a flow rate of 10 µl/s for 10 s, at intervals of 3 min. The swallowing
159 movement was identified using the electromyographic activity Power lab (AD
160 Instruments, Nagoya, Japan) and visual observation of the characteristic laryngeal
161 movement. The number of swallows was counted for 10 s after the injection of distilled
162 water, and the mean of the two measurements was expressed. The latency to swallowing

163 onset, which was defined as the time required to elicit the first swallow from the onset of
164 stimulation, was analyzed.

165

166 **Analysis of laryngeal residue**

167 We examined the area of the larynx mucosae, stained with pyocyanin blue, to determine
168 whether penetration or aspiration had occurred. At 6 days, the water bottle was changed
169 to a 0.025% pyoktanin aqueous solution (Honzo co. Ltd. Nagoya, Japan) after 16 h water
170 restriction, and animals were allowed to drink freely for 24 h. At 7 days, the animals were
171 sacrificed, and the larynx and trachea were harvested from each group. We measured the
172 percentage of stained area surrounding the epiglottis, aryepiglottic fold and interarytenoid
173 fold in the axial direction. Photographs of the tissues were captured for the larynx and
174 trachea, and the stained area was measured using ImageJ software
175 (<http://rsb.info.nih.gov/ij/>). Dividing the images into three primary colors, the white area
176 in the image obtained was quantified by subtracting red from blue and excluding green.

177

178 **Histomorphological analysis**

179 At 7 days after surgery, nerve-injured segments were harvested and fixed with 2.5%
180 glutaraldehyde (TAAB Laboratories Equipment Ltd., Reading, Berkshire, United
181 Kingdom) overnight at 4 °C. The nerve segments were subsequently fixed in 2% osmium
182 tetroxide (OsO₄; TAAB Laboratories Equipment Ltd.) for 2 h, separately dehydrated in
183 an ethanol gradient (50%, 70%, 80%, 90%, 95% and 100%), and treated in a gradient of
184 EPON812 (33%, 50%, 66% and 100%; TAAB Laboratories Equipment Ltd.) in propylene
185 oxide (Nacalai Tesque, Inc., Kyoto, Japan). Tissues were embedded in EPON812 in a 60
186 °C oven for 48 h. Semi-thin sections (200 μm) were cut vertically with an ultramicrotome
187 (Ultracut S; Leica Microsystems, Wetzlar, Germany), stained with 1% toluidine blue
188 solution, and examined under a light microscope (BZ9000; Keyence). The density of the
189 myelinated fibers (fibers/1000 mm²) was analyzed in five non-overlapping visual fields

190 per specimen. Ultrathin sections (70–80 nm) were cut with an ultramicrotome. We chose
191 axons exhibiting an equivalent diameter and evaluated the G-ratio as the ratio of the inner
192 axonal diameter to the total outer diameter. The stained samples were observed under
193 TEM (JEM-1400EX; JEOL Ltd., Tokyo, Japan). We randomly selected five separate
194 fields per slice for analysis.

195

196 **Immunohistochemical analysis**

197 Rats were deeply anesthetized before undergoing intracardiac perfusion with 4%
198 paraformaldehyde. The SLNs were isolated and embedded in OCT compound (Sakura
199 Finetek, Tokyo, Japan), and 20 μm sagittal sections were generated with a cryostat (Leica
200 CM3050S, Leica Biosystems, Denver, CO). The sections were permeabilized with 0.1%
201 Triton X-100 in phosphate buffered saline for 20 min, blocked with 5% bovine serum for
202 30 min and incubated overnight with the following primary antibodies: mouse anti-rat
203 CD31 (1:40, 550300 BD Pharmingen), rabbit anti-CD206 (1:1000, ab64693, Abcam) and
204 mouse anti-CD11b (1:1000, ab33827, Abcam). The following secondary antibodies were
205 used: anti-mouse IgG Alexa Fluor 488 and anti-rat IgG Alexa Fluor 647. After
206 counterstaining with 4',6-diamidino-2-phenylindole (DAPI, Sigma-Aldrich), tissue
207 images were observed through a universal fluorescence microscope (BZ9000; Keyence
208 Co., Osaka, Japan).

209

210 **Tissue preparation and qRT-PCR**

211 Cervical dislocation was used to kill the animals at 1, 3 and 7 days after injury. The SLNs
212 were harvested from animals in different groups and stored at $-80\text{ }^{\circ}\text{C}$. Total RNA was
213 isolated from the tissues using TRIZOL reagent (Invitrogen, Carlsbad, California)
214 according to the manufacturer's protocol. A spectrophotometer was used to quantify total
215 RNA levels, and RNA integrity was checked on 1% agarose gels. Reverse transcription
216 reactions were performed with Superscript IV reverse transcriptase (Invitrogen, Carlsbad,

217 California) using 0.1 µg total RNA in a 25 µl total reaction volume. The quantitative real-
218 time polymerase chain reaction (qRT-PCR) was performed using THUNDERBIRD
219 SYBR qPCR Mix (Toyobo, Osaka, Japan) and the Mx3000P QPCR System (Agilent
220 Technologies, Tokyo, Japan). The specific primers were designed using Primer3 (S1
221 Table). All results are normalized to glyceraldehyde 3-phosphate dehydrogenase
222 (GAPDH).

223

224 **Statistical analyses**

225 Statistical analyses were performed using SPSS for Windows, version 19.0 (IBM, New
226 York, USA). An unpaired two-tailed Student's t test was used when comparing two
227 groups. To analyze three or more independent groups, we used a one-way analysis of
228 variance (ANOVA), followed Tukey's *post hoc* test. Differences were considered
229 statistically significant at $p < 0.05$.

230

231 **Results**

232 **A novel visceral nerve lesion model with dysphagia in the rat was** 233 **established, and SHED-CM was found to improve dysphagia in this** 234 **model**

235 To elucidate the influence of the nerve lesion, we first measured food intake and body-
236 weight change in a novel animal model of bilateral SLN injury for 7 days. The food intake
237 and body-weights of the rats were significantly reduced after the SLN injury (Fig 1A).
238 Systemic delivery of the SHED-CM resulted in significantly less weight loss compared
239 to the Dulbecco's Modified Eagles' Medium (DMEM (-)) group. Similarly, food intake
240 in the SHED-CM group was increased compared to the DMEM (-) group.

241 To determine whether the SLN lesion could affect swallowing behavior in the rat, we
242 measured the volume of water intake, the number of swallowing interruptions, and the
243 lick rate using 2 min-long video recordings (S2 Video). We counted the number of

244 interruptions, defined by both the number of the head movements of the animal when in
245 drinking position and the number of failures to touch the tip of the water bottle when
246 licking. Licking is the primary way of ingesting liquids and consists in pressing the tongue
247 against the liquid, defined as the oral stage of swallowing [20, 21, 24]. Lick rate indicates
248 the rate of ingestion of liquid into the oral cavity of the rat [24]. The water intake per body
249 weight (ml/kg) decreased in the injury group compared to the sham group (Fig 1B).
250 Following the SLN lesion, the number of interruptions increased and the lick rate was
251 reduced (Fig 1C, 1D). Systemic delivery of SHED-CM significantly reduced the number
252 of interruptions, and increased the lick rate and water intake compared with the DMEM
253 (-) group. These results demonstrate that the SLN lesion caused dysphagia in the oral
254 stage of swallowing in the rat, and SHED-CM improved dysphagia in this stage.

255

256 **SHED-CM protects the swallowing reflex**

257 Next, we investigated whether SHED-CM promotes functional recovery after SLN injury.
258 Fig 2A shows examples of electromyographic activity recordings from the mylohyoid
259 muscle during distilled water administration into the pharyngeal region. The mean
260 number of swallows was significantly reduced in the injury group compared to the sham
261 group (Fig 2B). The latency to the first swallow was significantly extended in the injury
262 group compared to the sham group (Fig 2C). These results show that the volume of water
263 required to evoke the swallowing reflex was increased after SLN injury in the rat.
264 Administration of the SHED-CM significantly increased the number of swallows, and
265 shortened the latency to the first swallow compared with DMEM (-) (Fig 2B, 2C). A
266 comparison of the swallowing reflex among the SHED-CM group and DMEM (-) group
267 showed that the administration of SHED-CM improved the swallowing reflex and
268 enhanced functional recovery of the SLN. There were no significant differences between
269 the sham and SHED-CM groups with regard to the mean number of swallows and the
270 latency to the first swallow.

271

272 SHED-CM reduces pharyngeal residue

273 To determine whether the SLN lesion affected the pharyngeal stage of swallowing, we
274 investigated the laryngeal residue in the rat larynx. It is well known that the amount of
275 laryngeal residue is a predictor of aspiration and penetration in humans [25]. Previous
276 studies revealed that bilateral SLN injury in pigs affected swallow function and increased
277 aspiration incidence [26]. However, the impact of SLN injury in the rat was not reported.
278 Fig 3A shows an example of the larynx, and we measured the percentages of the larynx
279 and vocal cord areas that were stained. The stained areas in the larynx and vocal cord
280 were expanded in the injury group compared to the sham group (Fig 3B). Administration
281 of SHED-CM reduced the stained area in the larynx and vocal cord when compared with
282 DMEM (-) (Fig 3C). These results demonstrate that the SLN lesion caused dysphagia in
283 the pharyngeal stage of swallowing in the rat. Moreover, SHED-CM prevented water
284 storage in the pharynx, and might reduce the risk of aspiration and penetration. Staining
285 was not observed in the trachea and lungs in either group.

286

287 SHED-CM promotes axon regeneration after SLN injury

288 To examine nerve regeneration, we performed a histological analysis of the SLN in the
289 middle of the damaged area, 7 days after nerve injury. Examples of toluidine blue staining
290 and transmission electron microscopy (TEM) of the SLN cross-sectionally are shown in
291 Fig 4A. The toluidine blue staining showed widespread, severe edema, as well as
292 inflammation and Wallerian degeneration in the injury and DMEM (-) groups. TEM
293 showed that the typical structure of the nerve fibers almost disappeared in the injury and
294 DMEM (-) groups (Fig 4B). In contrast, many nerve myelinated fibers were identified in
295 the SHED-CM group (Fig 4A, 4B). Quantitative TEM analysis showed that the fiber
296 densities in the injury group were significantly lower than in the sham group (Fig 4C).
297 The mean G-ratio, the ratio between the inner and outer diameter of the myelin sheath,

298 was significantly higher in the injury group compared to the sham group. Meanwhile, the
299 SHED-CM group showed higher fiber densities when compared with the DMEM (-)
300 group (Fig 4C). Furthermore, the mean G-ratio showed that the degree of myelination in
301 the SHED-CM group was significantly higher compared to the DMEM (-) group (Fig 4D).
302 There were no significant differences between the sham and SHED-CM groups with
303 regard to the fiber density and G-ratio. In addition, we counted myelinated fibers with an
304 axon diameter of less than 5 μm and measured the G-ratios of these myelinated fibers. In
305 a previous study, myelinated fibers with less than 5 μm of diameter in the SLN were
306 classified as A- β fibers [27]. The number of A- β fibers in the SHED-CM group was
307 significantly increased compared to the DMEM (-) group (Fig. 4E). The G-ratio of A- β
308 fibers in the SHED-CM group was higher than in the DMEM (-) group (Fig 4F). These
309 results strongly suggest that SHED-CM promoted functional nerve regeneration
310 following the SLN lesion.

311

312 **SHED-CM recruits M2 macrophages at the injury site**

313 We examined the mRNA expression profiles of pro-inflammatory and anti-inflammatory
314 factors in the SLNs (Fig 5A). The administration of SHED-CM markedly suppressed the
315 expression of the pro-inflammatory mediators inducible nitric oxide synthase (iNOS) and
316 interleukin-1 beta (IL-1 β), and increased the expression of the anti-inflammatory M2
317 macrophage markers arginase-1 (Arg-1) and interleukin-10 (IL-10), at 1 day after injury.
318 Leukemia inhibitory factor (Lif) and chemokine C-C motif ligand (Ccl2), also known as
319 monocyte chemoattractant protein-1, contributed both to the attraction of macrophages to
320 the damaged nerve site and to nerve regeneration [28]. These chemokines were also
321 upregulated in the SHED-CM group at earlier time-points after nerve injury.
322 Immunohistochemical analysis showed an accumulation of M2 macrophages at the nerve
323 injury site 3 day after nerve injury (Fig 5B). Quantitative analysis revealed that the
324 number of CD11b macrophages in SHED-CM was increased relative to the DMEM (-)

325 group (Fig 5C). The proportion of CD11b/CD206-positive M2 macrophages was
326 significantly decreased in the SHED-CM group compared to the DMEM (-) group (Fig
327 5D). These results demonstrate that SHED-CM promotes M2 macrophage recruitment.

328

329 **SHED-CM upregulates trophic factors and promotes vascularization at** 330 **the injury site**

331 Nerve regeneration depends on the expression of neurotrophic factors [29, 30]. Systemic
332 administration of the SHED-CM upregulated levels of neurotrophic factors, including
333 nerve growth factor (NGF), brain-derived neurotrophic factor (BDNF) and neurturin
334 (NTN), and this upregulation peaked at 1 and 3 days after nerve injury (Fig 6A).
335 Furthermore, vascularization in the nerve injury site was investigated. qRT-PCR analysis
336 revealed that the mRNA expression of vascular endothelial growth factor (VEGF)
337 increased at 1, 3, and 7 days after nerve injury compared to the DMEM (-) group (Fig
338 6A). Immunostaining for the vascular endothelial cell marker CD31 showed that the
339 administration of SHED-CM considerably promoted vascular endothelial cell migration
340 towards the lesion site, as shown in the longitudinally sectioned samples at 7 days after
341 nerve injury (Fig 6B). Quantitative analysis showed that the area of blood vessels in the
342 nerve lesion site was significantly increased in the SHED-CM group compared with the
343 DMEM (-) group (Fig 6C). These results suggest that SHED-CM promotes nerve
344 regeneration via vascularization.

345

346 **Discussion**

347 In the present study, we established a novel animal model of visceral nerve lesion that
348 allowed evaluation of rat swallowing function. Our experiments demonstrate that SLN
349 injury in the rat induced weight loss, and reduced food and water intake. Dysphagia
350 caused by the SLN injury also showed that there was a delayed swallowing reflex and
351 pharyngeal storage, indicating dysfunction of the oral and laryngeal stages of swallowing.

352 In addition, our results suggest that administration of SHED-CM following the SLN
353 injury improved swallow function and enhanced nerve regeneration through M2
354 macrophage polarization and vascularization. Here, we show that our novel animal model
355 of SLN injury can be used as a novel visceral nerve regeneration model, and that SHED-
356 CM may have therapeutic benefits for SLN injury.

357 Until now, the SLN was widely used in swallowing studies to evoke the swallowing reflex
358 [23, 31]. This study is the first to assess swallowing behavior in rodents following SLN
359 injury. Our study indicated that rats with dysphagia caused by SLNs lesion fail to consume
360 water continuously, and have a reduction in water consumption per unit of time. The
361 reduction in water intake following SLN injury suggests that rats can drink water in small
362 quantities for single swallowing. With regard to oropharyngeal evaluation, previous
363 studies found a correlation between the loss of sensory input from the laryngeal area and
364 the occurrence of penetration and aspiration in humans [32, 33]. Although the relationship
365 between sensory loss in laryngeal area and aspiration in the rat was not unraveled, our
366 data show that the removal of the stimulus from SLN to the larynx causes dysfunction in
367 the oral and laryngeal stages of swallowing.

368 Moreover, in previous animal studies, swallowing function was analyzed using
369 videofluoroscopic swallow study (VFSS) methods, which were considered the standard
370 gold method for assessing swallowing function clinically [20, 26, 34]. Although VFSS
371 makes it possible to observe, in detail, bolus flow in the oral, oropharyngeal, and
372 esophageal stages of swallowing, the use of VFSS in rats is not easy because of the high
373 swallowing speed of rodents, which is 10 times faster than humans' [20]. The method of
374 drinking the stain solution, used in our study, was a simple way to compare the degree of
375 laryngeal storage. Thus, our model allowed for the simple evaluation of dysphagia in the
376 pharyngeal stage of swallowing in the rat without VFSS.

377 A proper inflammatory response, namely macrophage phenotype-switching, is necessary
378 for tissue regeneration after peripheral nerve injury. Resident and infiltrating

379 macrophages and dedifferentiated Schwann cells remove axonal and myelin debris, and
380 create an environment for axonal regeneration [28, 35]. Recent studies have shown that
381 macrophages polarization from the M1 phenotype to the M2 phenotype induced by IL-4
382 and IL-10 contribute to axonal regeneration [36, 37]. Our findings showed that a single
383 systemic administration of SHED-CM suppresses pro-inflammatory M1 phenotype
384 macrophages, and activates anti-inflammatory M2 phenotype macrophages at the injury
385 site. However, the mechanism behind this transition remains unclear. In recent studies, it
386 was shown that depicting macrophages as having the ability to switch from one phenotype
387 to another phenotype is not quite accurate. Macrophages can change their functional
388 phenotype according to the microenvironment, and multiple cytokine treatment induced
389 multiple functional phenotypes of macrophages [38].

390 The gene expression pattern in this study showed that SHED-CM induced striking
391 changes in many parameters. In the damaged peripheral nerve, a pro-inflammatory
392 immune response is triggered, with Ccl-2 and Lif regulating macrophage recruitment [39,
393 40]. These factors are rapidly produced by Schwann cells, and infiltrating macrophages
394 produce a chemokine that stimulate the recruitment of even more macrophages [28].
395 Additionally, large numbers of macrophages in Wallerian degeneration in peripheral
396 nerve system are mostly recruited from bone marrow [35]. Our data show that the
397 administration of SHED-CM strongly upregulated Ccl-2 and Lif, resulting in a strong
398 attraction of macrophages to the injury site. Although it was difficult to completely
399 distinguish hematogenous macrophages from residential macrophages *in vivo*, the results
400 imply that SHED-CM recruited many hematogenous M2 polarized macrophages, and that
401 they infiltrated into the damaged SLN. Moreover, recent studies showed that neurotrophic
402 factors, including NGF, BDNF and NTN, are important for neuron growth and/or survival
403 [30, 41, 42]. The upregulation of these factors also indicates that SHED-CM promotes
404 tissue repair at the injury site.

405

406 Angiogenesis is a crucial process for tissue regeneration. In peripheral nerve regeneration
407 processes, Bungner's bands, which guide regenerating axons, are formed when axons
408 grow back to their target site following Wallerian degeneration [28]. New blood vessels
409 induced by VEGF-A, which is produced by macrophages under hypoxic conditions
410 within the nerve injury site, allow Schwann cells to migrate and contribute to the
411 formation of Bungner's bands [43]. Previous *in vitro* studies showed that SHED-CM
412 enhances Schwann cell proliferation and migration, and promotes tube formation by
413 human umbilical vein endothelial cells [17]. hDPSC had the high angiogenic
414 differentiation capabilities [44], and CM from hDPSCs also promotes endothelial cell
415 proliferation and growth [45]. Moreover, microvesicles derived from M2 macrophages
416 promoted nerve regeneration through proliferation and migration of Schwann cells [46].
417 Taken together, our results, plus the available evidence in the literature, suggest that
418 SHED-CM promotes Bungner's band formation via new blood vessel formation that
419 allows Schwann cells to migrate.

420 The VEGF contained in SHED-CM can be considered as a therapeutic candidate.
421 However, use of the VEGF requires for appreciate concentration, timing, and spatial
422 distribution owing to formation of vascular abnormalities [47]. Administration of high
423 doses VEGF without other trophic factors induced fragile and unstable vessels [48] [49].
424 Moreover, in a clinical trial, intracoronary and intravenous infusion of VEGF did not lead
425 to significant therapeutic benefits [50]. Therefore, we hypothesize that part of the
426 therapeutic effect of SHED-CM is due to factors related to the conversion of M1
427 macrophages to M2 macrophages, such as IL-4, IL-10, Ccl-2, and the secreted
428 ectodomain of sialic acid binding Ig-like lectin-9 (sSiglec-9). Administration of IL-4 or
429 IL-10 was shown to modulate the ratio of M1 and M2 macrophages [36, 37]. However,
430 the amount of these factors used in the study was higher than the amount present in
431 SHED-CM [18]. Furthermore, although administration of high doses of Ccl-2 and
432 sSiglec-9 (two molecules found in SHED-CM) elicited the same effect as SHED-CM in

433 functional nerve recovery, when these factors are administered at concentration similar to
434 those found in SHED-CM, they elicit insufficient improvement [51]. Additional studies
435 will be necessary to further investigate therapeutic factors in SHED-CM.

436 In this study, we developed a novel animal model of SLN injury that showed dysphagia
437 in the oral and laryngeal stages of swallowing in the rat. Administration of SHED-CM
438 improved functional recovery in our model, an effect that likely occurs through two
439 mechanisms: macrophage polarization and vascularization. Our study suggests that
440 SHED-CM may provide therapeutic benefits for patients with SLN injury.

441

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451

452

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642 **Supporting information**

643 **S1 Table. Primer sequences used for the qRT-PCR.**

644 **S1 Video. Comparison of swallowing behavior in video recordings.**

645

646 **Author Contributions**

647 **Conceptualization:** Takeshi Tsuruta, Kiyoshi Sakai, Wataru Katagiri, Hideharu Hibi.

648 **Data curation:** Takeshi Tsuruta, Junna Watanabe.

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650 **Funding acquisition:** Kiyoshi Sakai.

651 **Investigation:** Takeshi Tsuruta, Junna Watanabe.

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653 **Project administration:** Hideharu Hibi.

654 **Software:** Takeshi Tsuruta.

655 **Supervision:** Hideharu Hibi.

656 **Validation:** Kiyoshi Sakai.

657 **Visualization:** Kiyoshi Sakai.

658 **Writing – original draft:** Takeshi Tsuruta.

659 **Writing – review & editing:** Kiyoshi Sakai, Hideharu Hibi.

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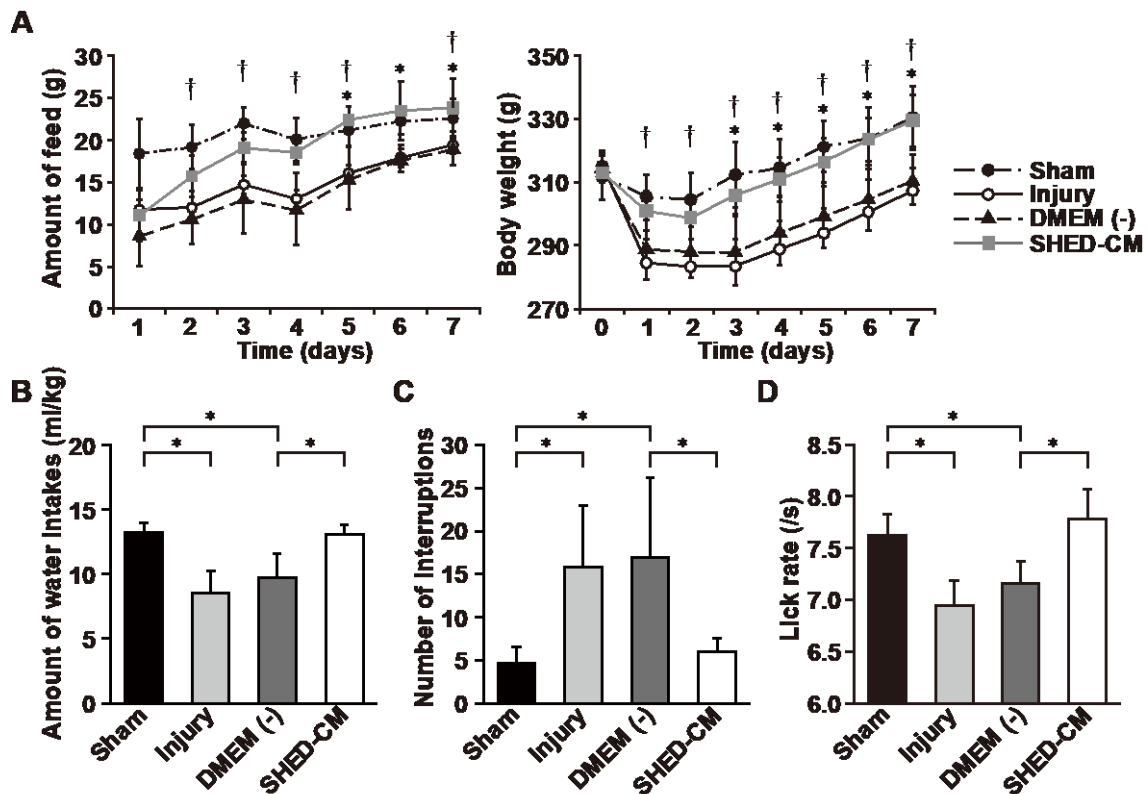
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Fig 1. A novel model with dysphagia in the rat was established, and SHED-CM was found to improve dysphagia.

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(A) Graph showing food intake and body-weight change after SLN injury. $n=6$ per group. † $p < 0.05$, sham group versus injury group; * $p < 0.05$, DMEM versus SHED-CM group. Results are presented as mean \pm SEM. (B–D) Analysis of swallowing behavior using non-radiographic video recording for 2 min. (B) Measurement of the volume of water intake per body-weight (ml/kg). (C) Measurement of interruptions during swallowing behavior. (D) Measurement of lick rate for 2 min. $n=6$ per group. * $p < 0.05$. Results are presented as mean \pm SEM.

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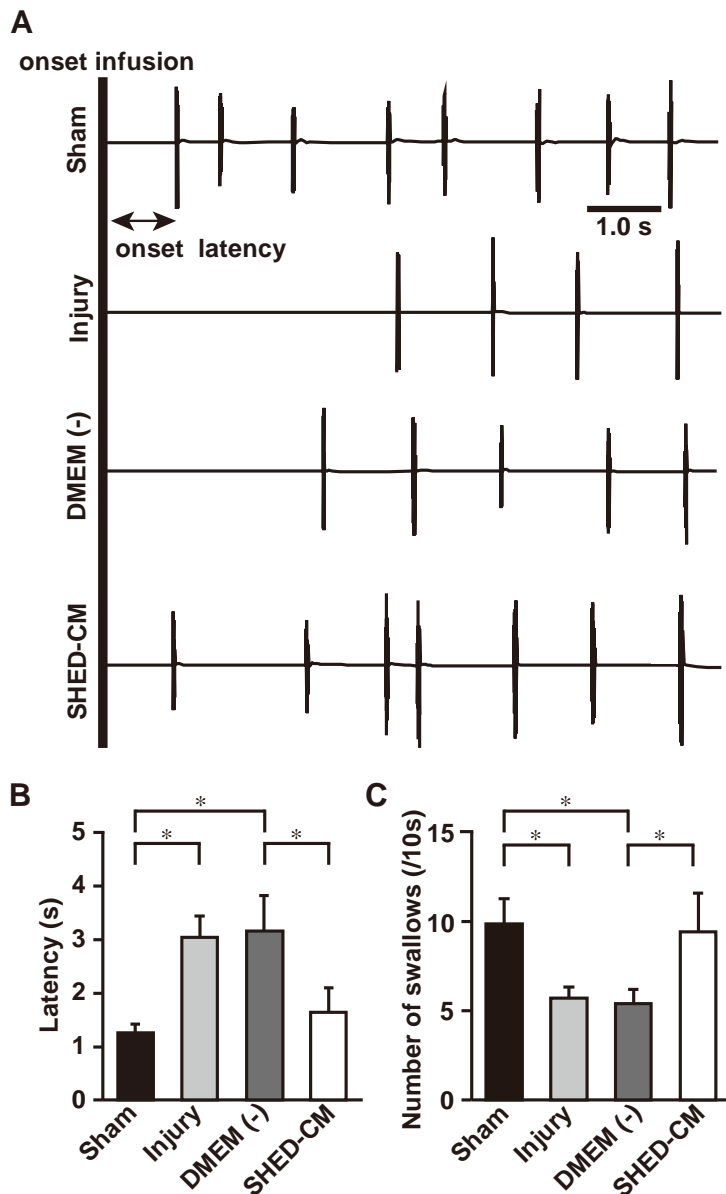
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Fig 2. Effects of SHED-CM administration on swallowing initiation.

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(A) Representative electromyographic recordings from the mylohyoid muscle during swallowing.

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Measurement of the mean number of swallows (B) and the onset latency to the first swallow (C). SLN

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injury affects the number of swallows and the latency to swallow. SHED-CM improves the number of

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swallows and the latency to swallow relative to DMEM (-). n=6 per group. *p < 0.05. Results are

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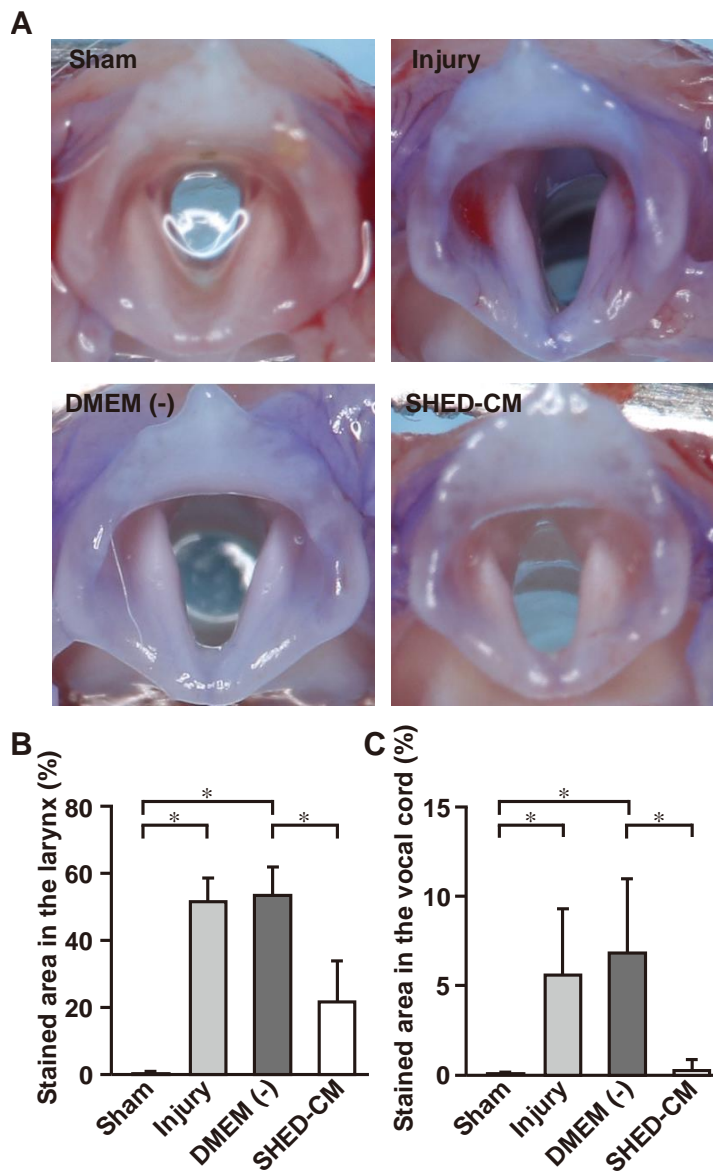
presented as mean \pm SEM.

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697 **Fig 3. Quantification of the extent of staining in the larynx.**

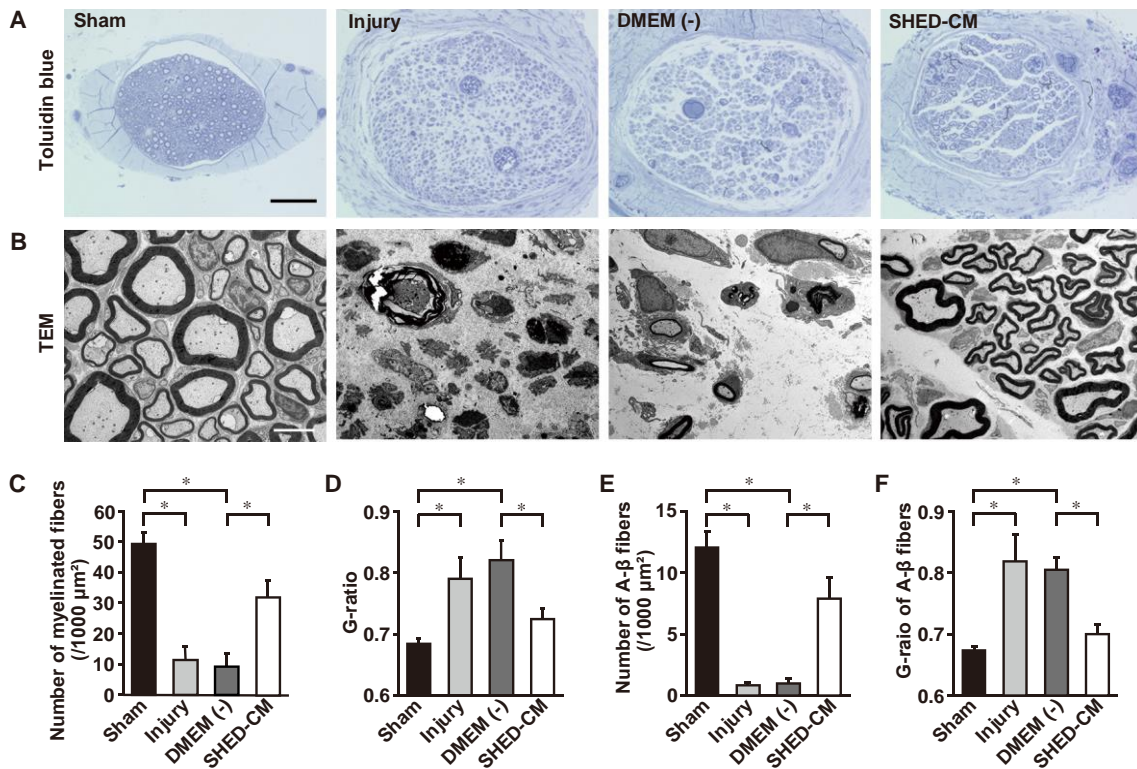
698 (A) Representative image of the larynx in each group, at 7 days after SLN injury. Analysis of the
 699 stained area in the larynx (B) and in the vocal cord (C). The stained area in the larynx and vocal cord
 700 increases after SLN injury. Treatment with SHED-CM significantly reduces the stained area in the
 701 larynx and vocal cord relative to DMEM (-). n=6 per group. *p < 0.05. Results are presented as mean
 702 ± SEM.

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708 **Fig 4. Morphological evaluation of nerve regeneration in the SLN.**

709 (A) Toluidine blue staining of semi-thin sections from the middle of the injury segments at 7 days after
 710 SLN injury. Scale bar 50 μm . (B) TEM images of ultrathin cross sections of segments from the middle
 711 of the injury at 7 days after SLN injury. Scale bar: 5 μm . The injury group shows widespread
 712 inflammation and Wallerian degeneration at 7 days after SLN injury. Analysis of myelinated fiber
 713 densities (C) and the G-ratio (D). Myelinated fiber densities and the G-ratio in the SHED-CM group
 714 significantly improve relative to the DMEM (-) group. Analysis of A- β fiber densities (E) and the G-
 715 ratio of the A- β fibers (F). The densities and the G-ratios of the A- β fibers are significantly higher in
 716 the SHED-CM group than in the DMEM (-) group. $n=6$ per group. $*p < 0.05$. Results are presented as
 717 mean \pm SEM.

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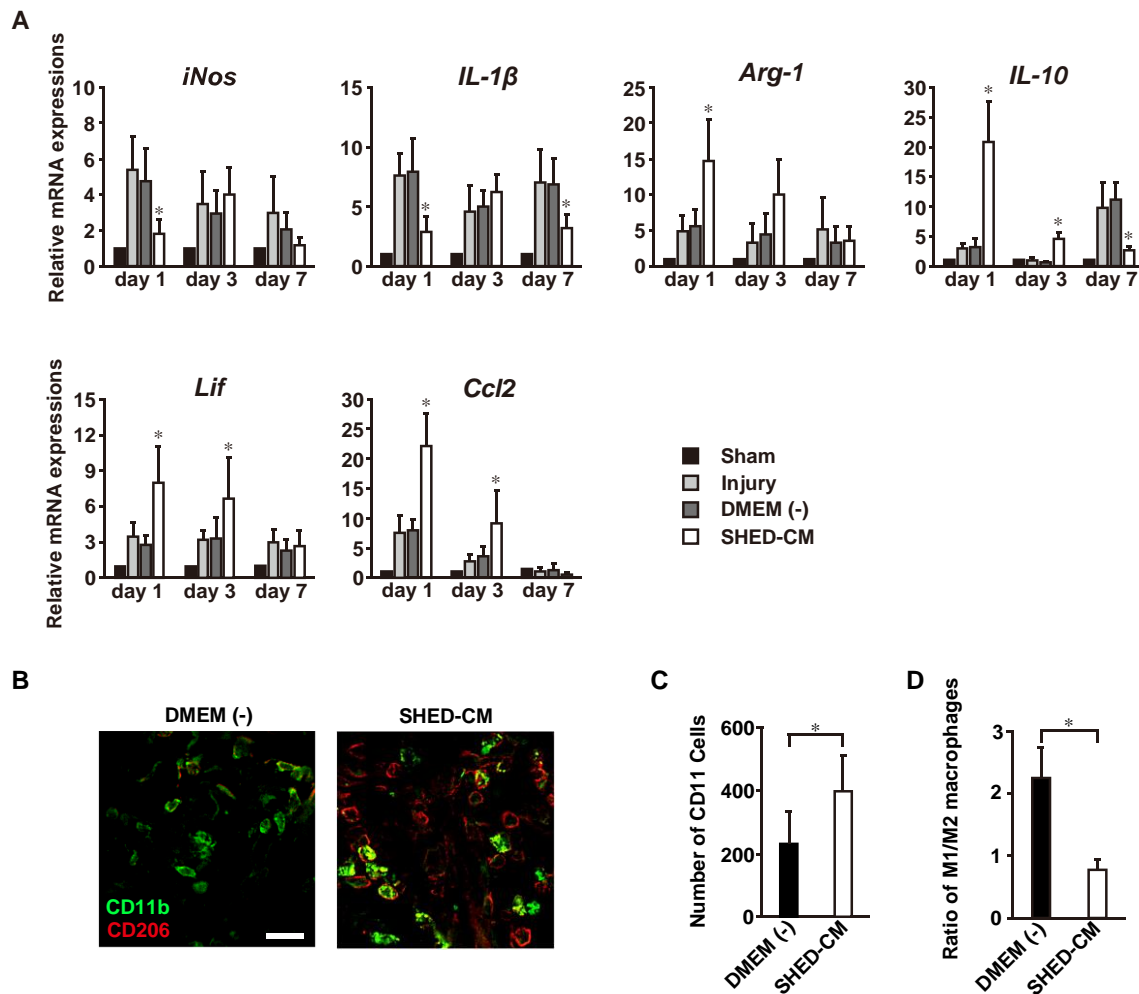
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726 **Fig 5. SHED-CM recruits M2 macrophages to the injury site.**
727 (A) SHED-CM administration downregulates M1 markers (*iNos*, *IL-1 β*) and upregulates M2 markers
728 (*Arg-1*, *IL-10*). SHED-CM also suppresses the expression of *IL-6*, and upregulates *Lif* and *Ccl2*.
729 Results are expressed relative to the level in the sham-operated model. All results are normalized to
730 GAPDH. $n = 6$ per group. $*p < 0.05$. Results are presented as mean \pm SEM. (B) Representative images
731 of the immunohistological staining of D206 and CD11b. (C) Quantification of CD11b macrophages
732 at injury site. (D) The proportion of CD11b/CD206-positive macrophages. $n = 6$ per group. $*p < 0.05$.
733 Results are presented as mean \pm SEM. Scale bar in (B): 20 μ m.

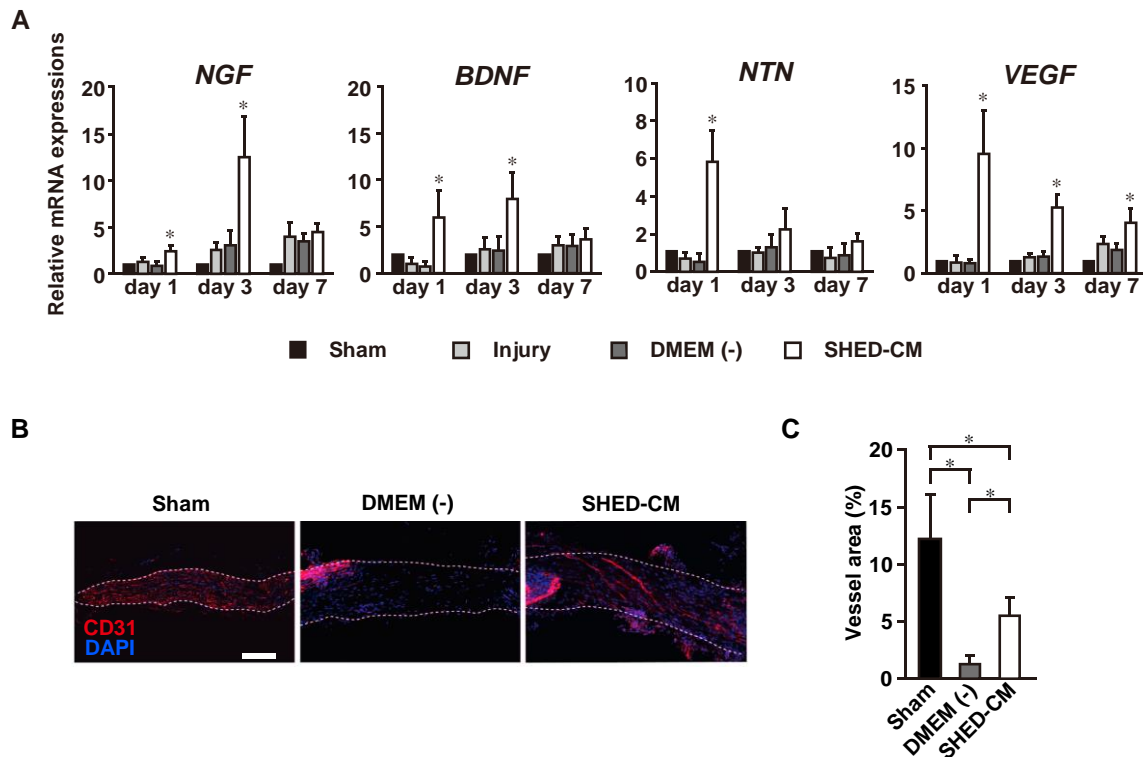
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740 **Fig 6. SHED-CM promotes vascularization and recruits M2 macrophages to the injury site.**

741 (A) SHED-CM upregulates the expression of multiple trophic factors. Results are expressed relative
 742 to the level in the sham-operated model. All results are normalized to GAPDH. $n = 6$ per group. $*p <$
 743 0.05 . Results are presented as mean \pm SEM. (B) Representative images of the immunohistological
 744 staining of CD31 in a sagittal section of the SLN at 7 days following the SLN lesion. (C) Quantification
 745 of CD31 cells in the injury site. SHED-CM significantly enhances the area of blood vessels in the
 746 nerve lesion site compared to DMEM (-). Scale bar in (B): $100 \mu\text{m}$. $n = 6$ per group. $*p <$
 747 0.05 . Results are presented as mean \pm SEM.

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